



WALKMECH

ENERGY-EFFICIENT TRANSFEMORAL PROSTHESIS

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OUTLINE

- THE PROBLEM
- THE CLASSIFICATION
- PROPOSED CONCEPT
- WORKING PRINCIPLE
- THE REALIZATION
- TESTS
- RESULTS
- CONCLUSIONS



THE PROBLEM

transfemoral prosthesis

Amputation level	Energy above healthy subject [%]	Speed [m/min]
Long transtibial	10	70
Average transtibial	25	60
Short transtibial	40	50
Bilateral transtibial	41	50
Transfemoral	<u>65</u>	40
Wheelchair	0-8	70

THE CLASSIFICATION

transfemoral prosthesis – passive



MAUCH GM - Ossur



MAUCH XG - Ossur



Total Knee 2100 - Ossur



3R95 - Otto Bock



3R80 - Otto Bock

THE CLASSIFICATION

transfemoral prosthesis



C-Leg & C-Leg compact – Otto Bock



Rheo Knee – Ossur



Smart Adaptive – Endolite

THE CLASSIFICATION

transfemoral prosthesis



Power Knee - Ossur

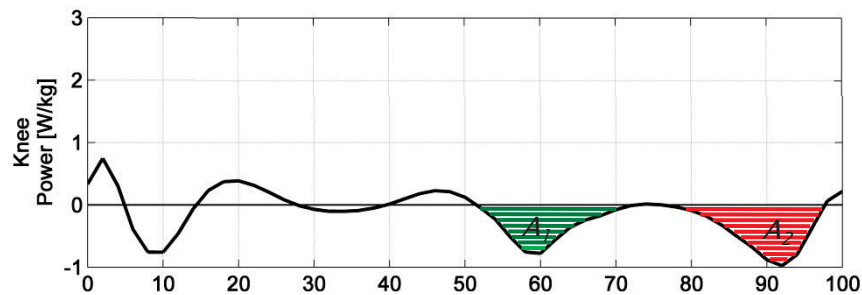
THE CLASSIFICATION

transfemoral prosthesis

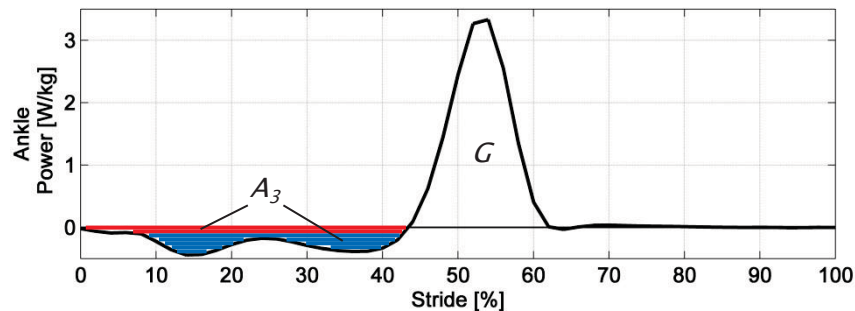
Passive	MP Controlled	Powered
- No speed adaptation	+ Adaptive walking	+ Adaptive walking
- No push off	- No push off	+ Push off support
- High metabolic cost	- High metabolic cost	+ Reduced metabolic cost
+ No battery	Requires batteries	- Big batteries
+ Low price	Medium price	- High price

PROPOSED CONCEPT

in theory walking is almost energy free...



$$A_1 + A_2 \\ \sim 0.20 \text{ J/kg}$$



$$A_3 \\ \sim 0.13 \text{ J/kg}$$

$$G \\ \sim 0.35 \text{ J/kg}$$

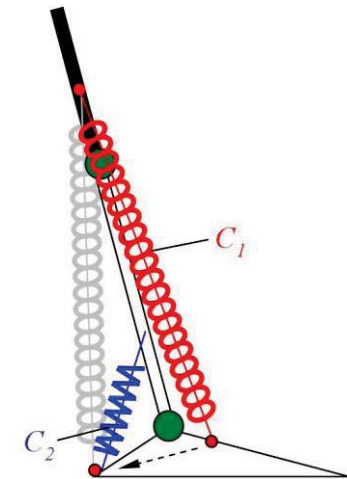
PROPOSED CONCEPT

in theory walking is almost energy free...

to design an actuation system;

- that is able to **store** (power absorption) and **release** the energy (power generation)
- that provides **energy exchange** between the knee and ankle joints.

The actuation system is to be controlled without dissipation (**brakes**) and will make use of every joule of energy during walking cycle (**energy efficient**).

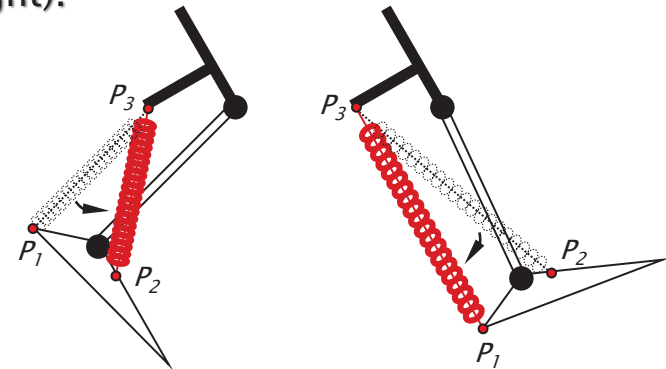
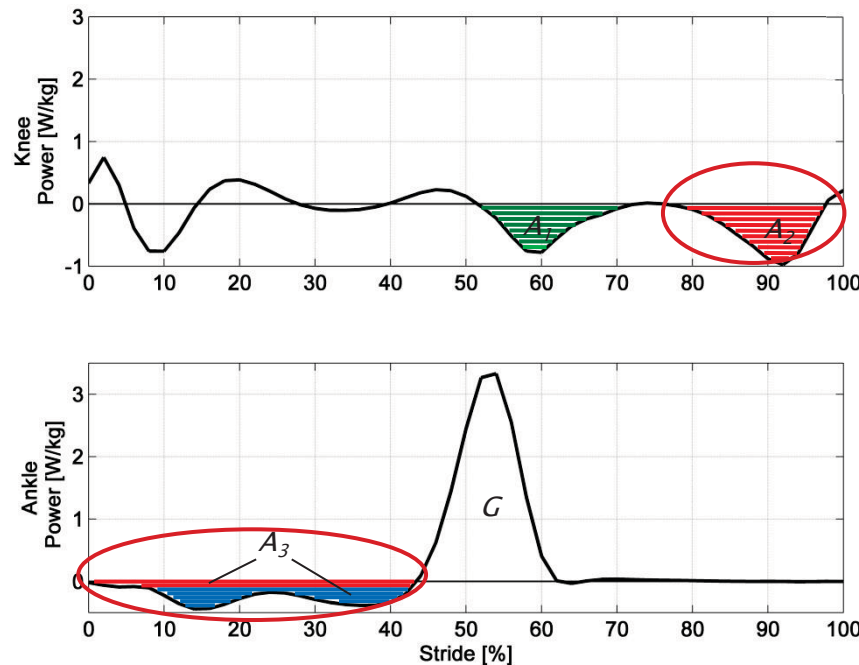


WORKING PRINCIPLE

bi-directional element

After pre-swing phase, the attachment point of the spring is changed from the heel (P_1) to the upper part of the foot (P_2) (left).

At the end of the swing, the spring is loaded and its position changes back to the P_1 (right).

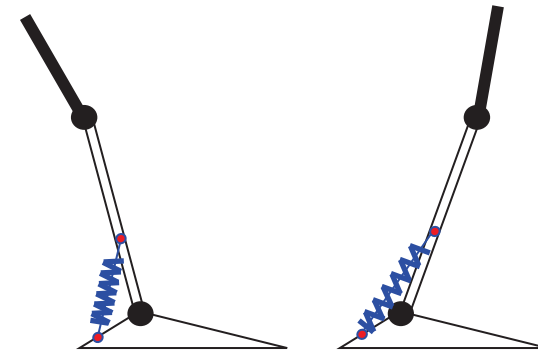
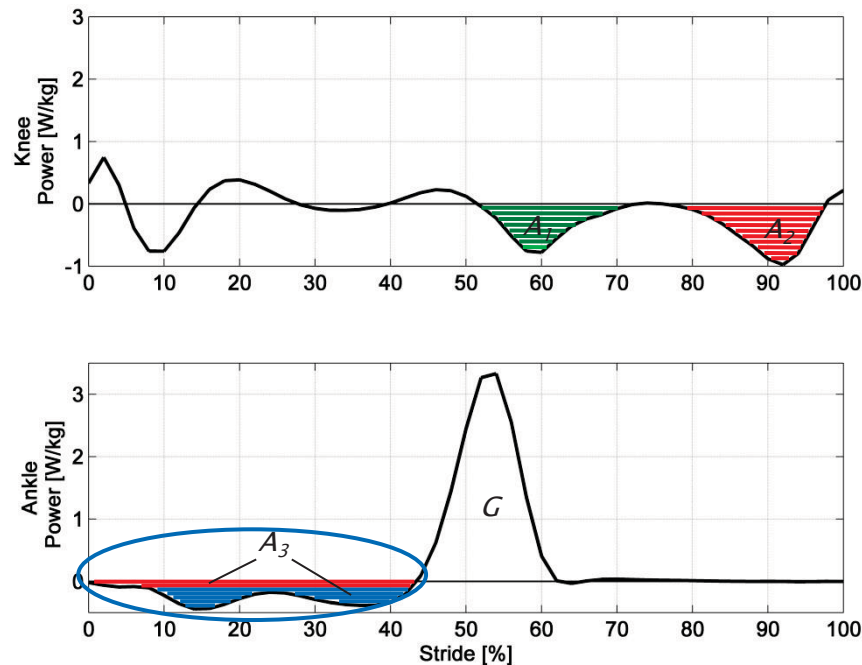


WORKING PRINCIPLE

ankle elastic element

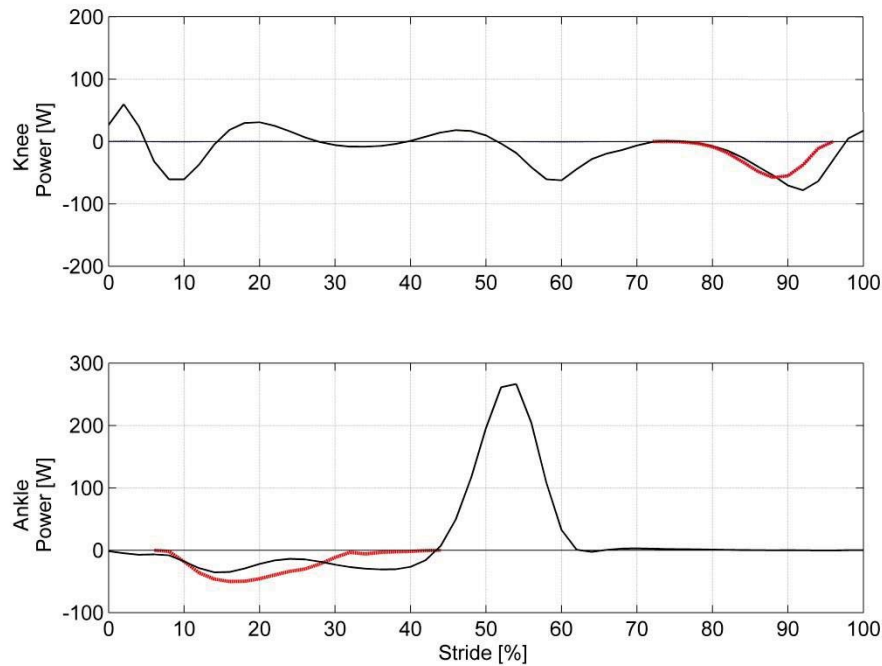
At the beginning of the stance phase, both elements C_2 and C_3 are ready for the storage of absorption A_3 (left).

At the end of the stance phase, both springs are loaded (right).



SIMULATIONS

power flow for each joint

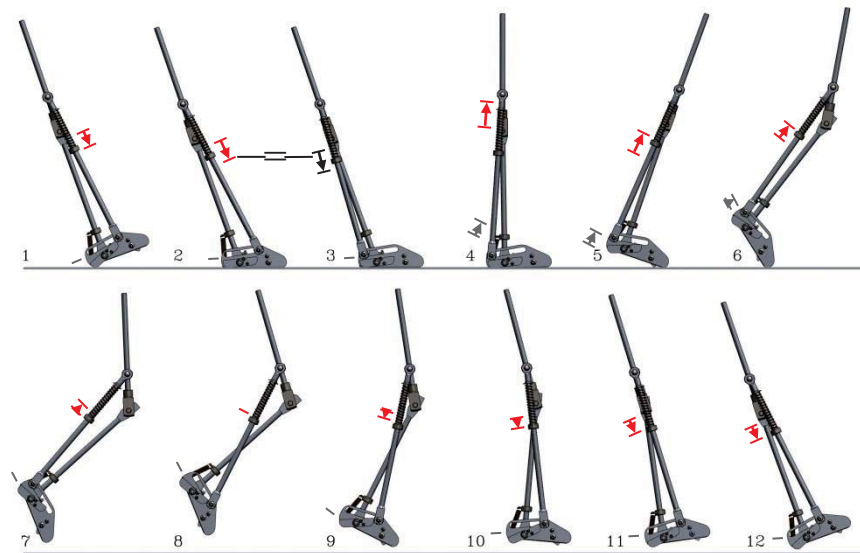


64% overall system efficiency



THE REALIZATION

Energy is stored, exchanged and released

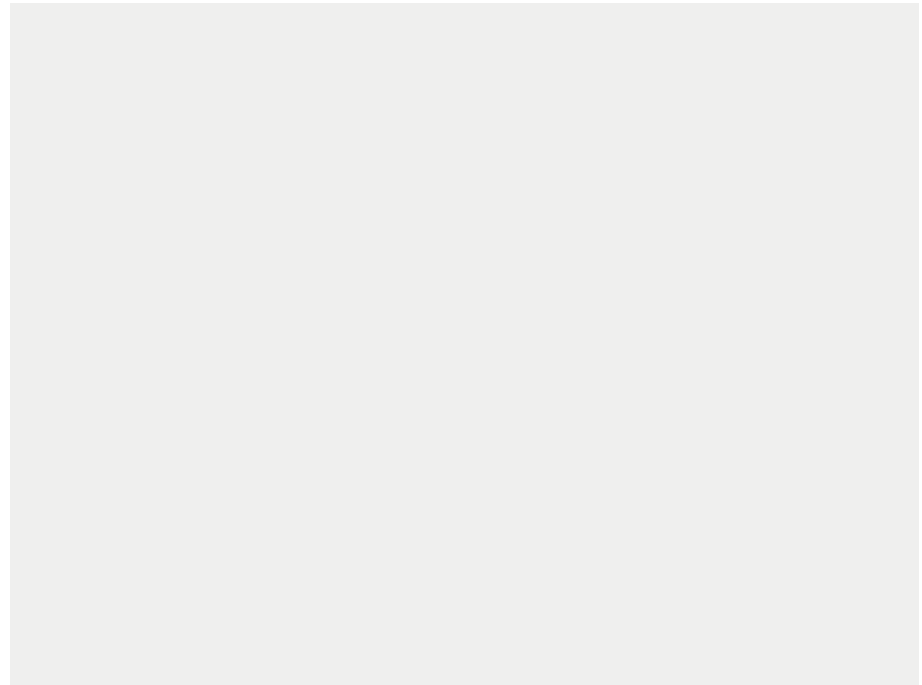


TESTS

set-up

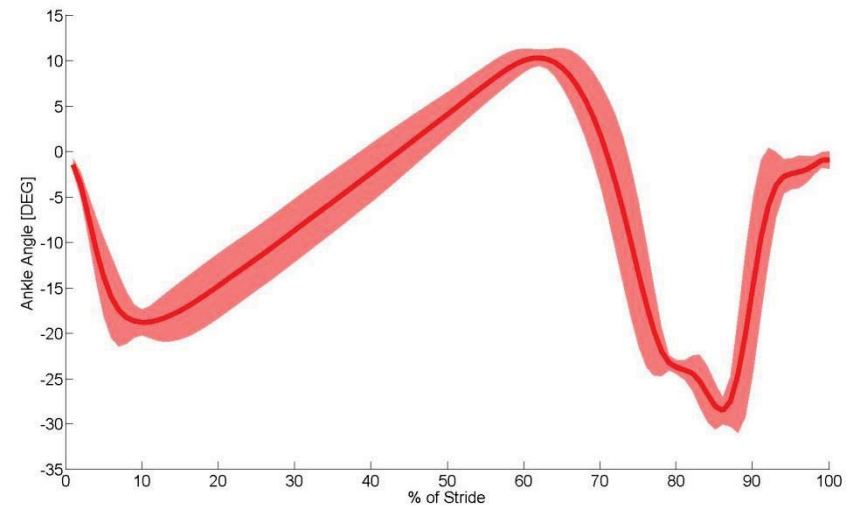
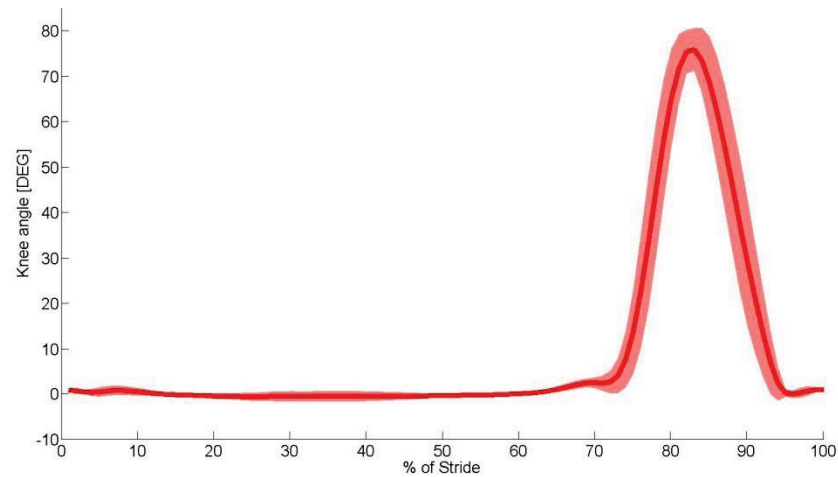
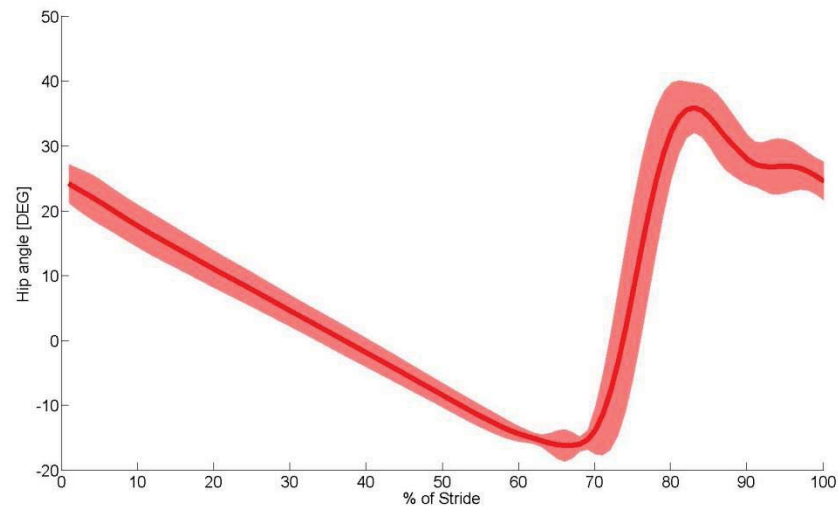


TESTS



RESULTS

joint angles

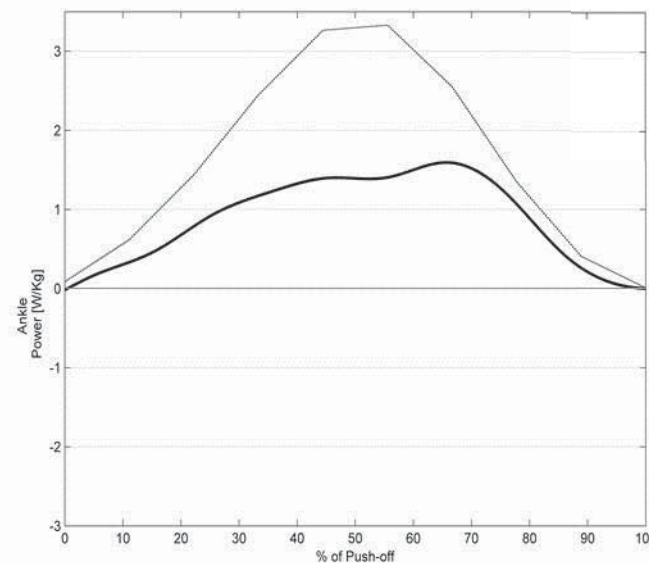
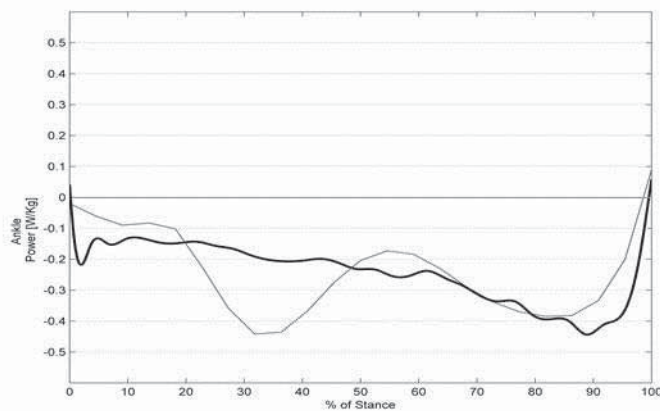
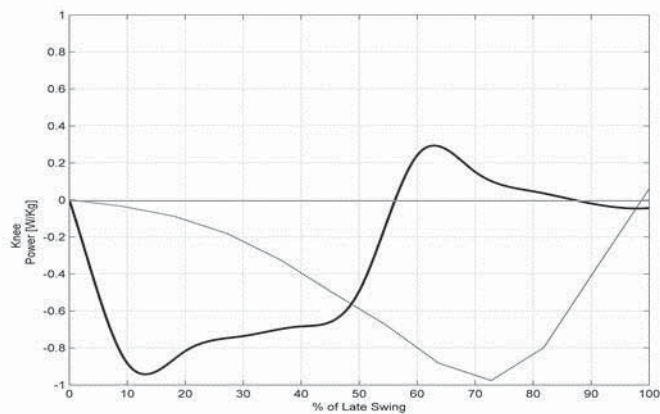


RESULTS

joint power

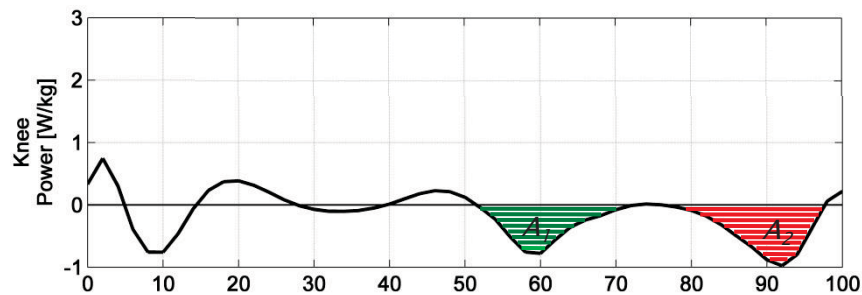
Almost all of A_2 portion is stored

50% of push-off is provided

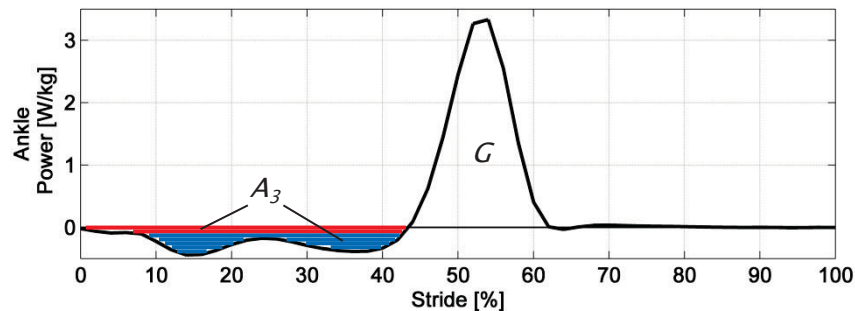


PROPOSED CONCEPT – II

in theory walking is almost energy free...



$$A_1 + A_2 \\ \sim 0.20 \text{ J/kg}$$

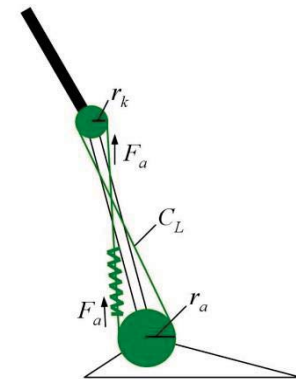
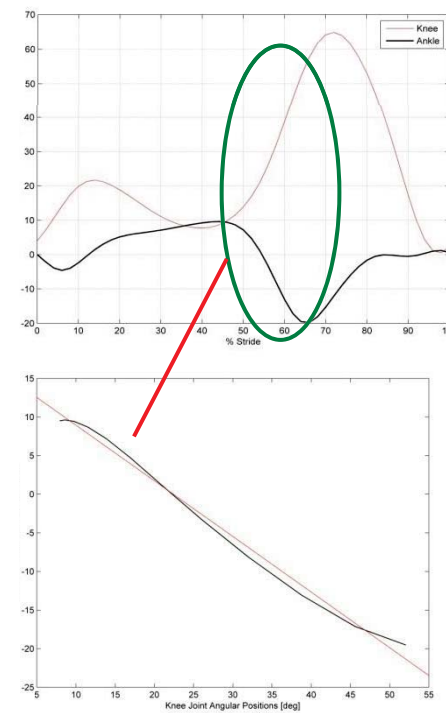
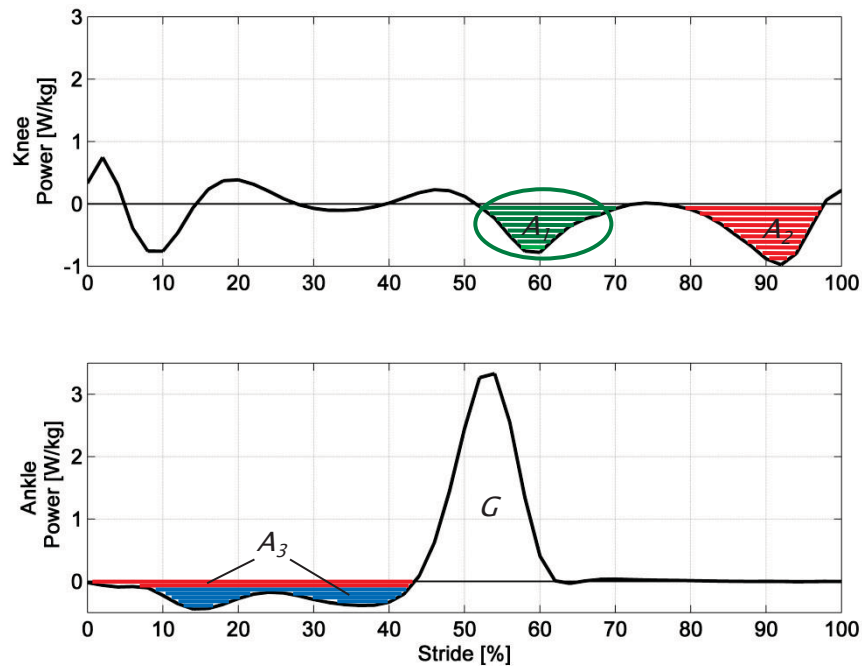


$$A_3 \\ \sim 0.13 \text{ J/kg}$$

$$G \\ \sim 0.35 \text{ J/kg}$$

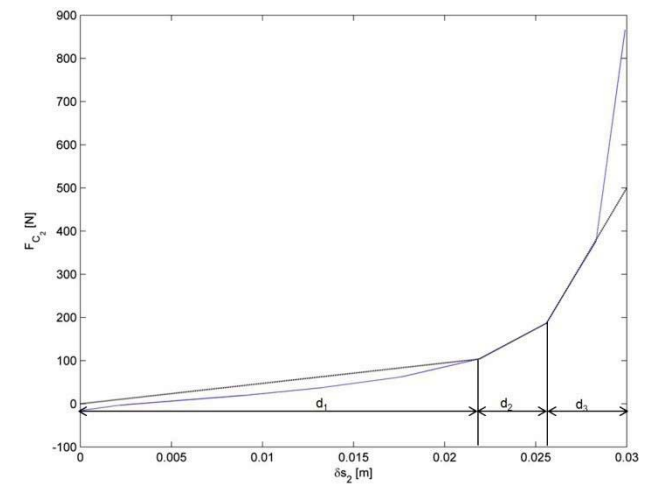
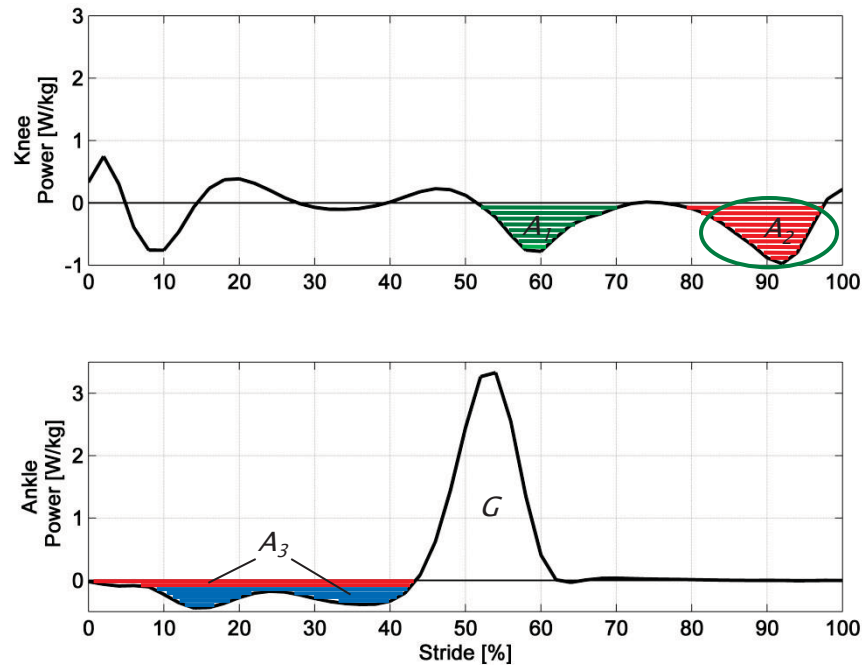
WORKING PRINCIPLE

linkage element



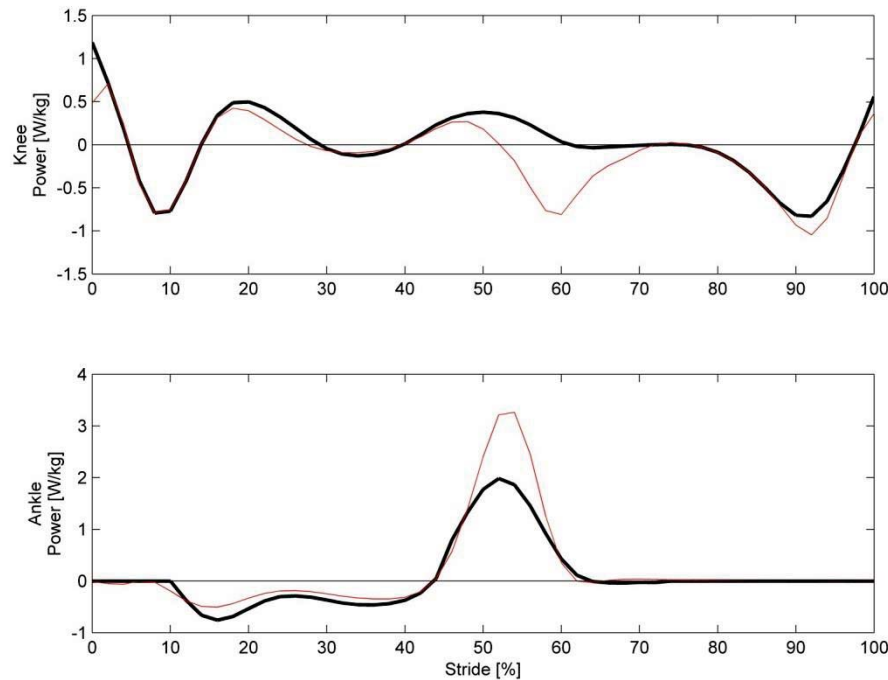
WORKING PRINCIPLE

progressive element



SIMULATIONS

power flow for each joint

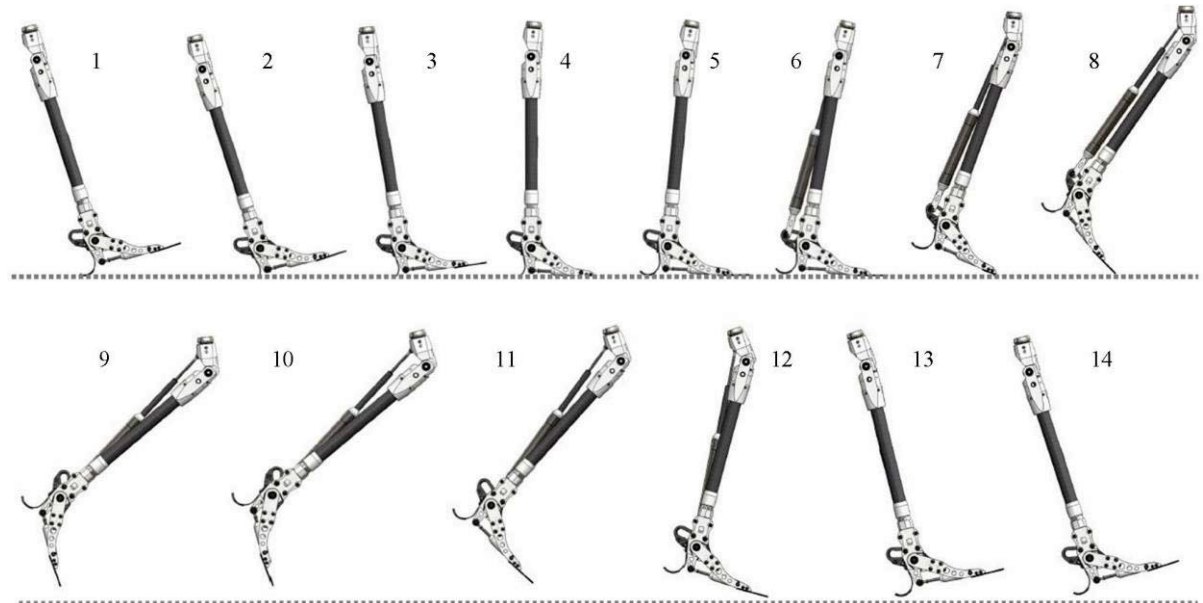


76% overall system efficiency



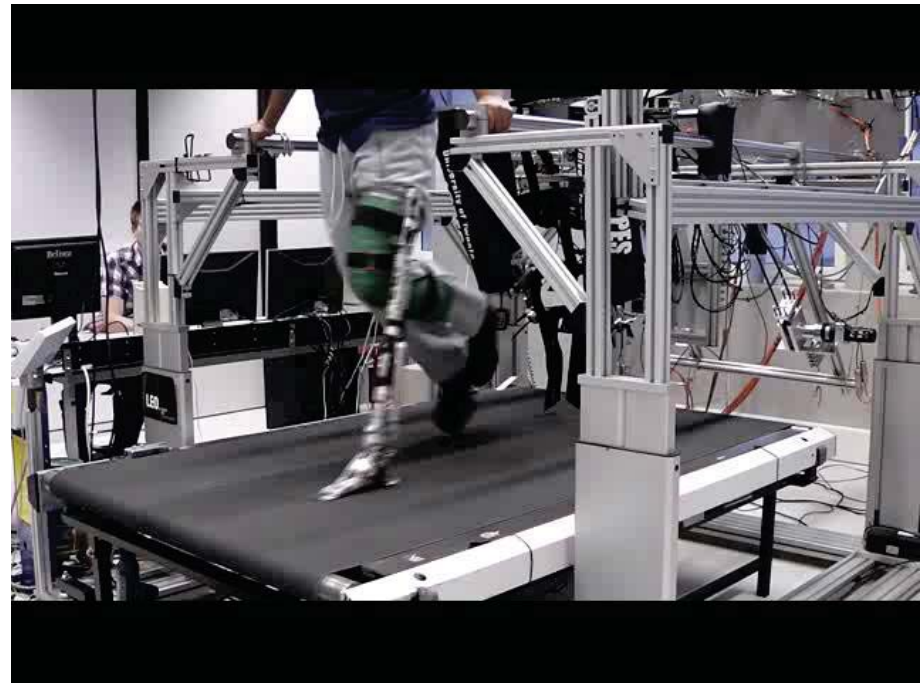
THE REALIZATION

Energy is stored, exchanged and released



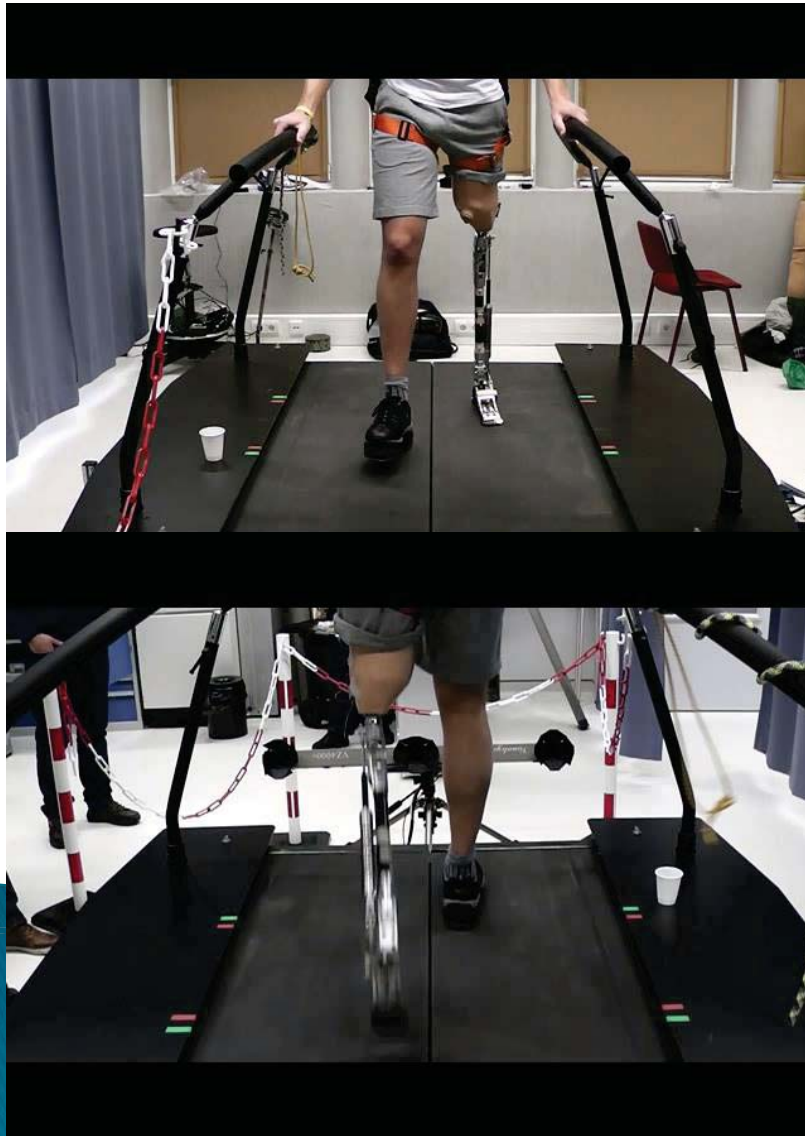
TESTS

healthy subjects



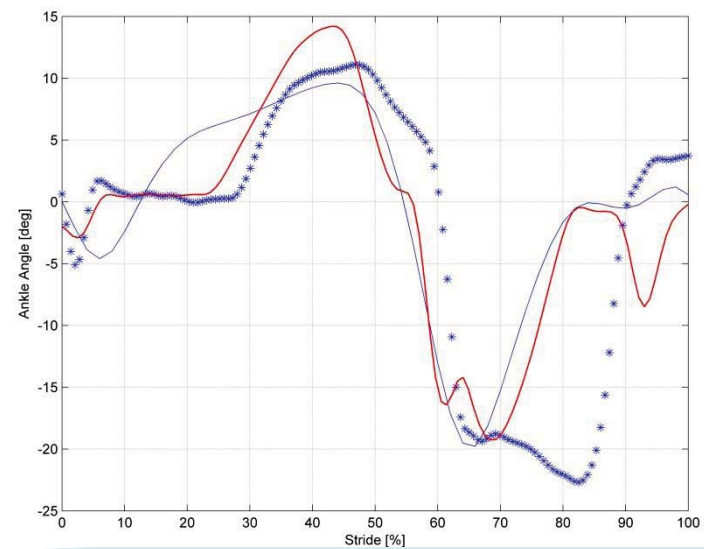
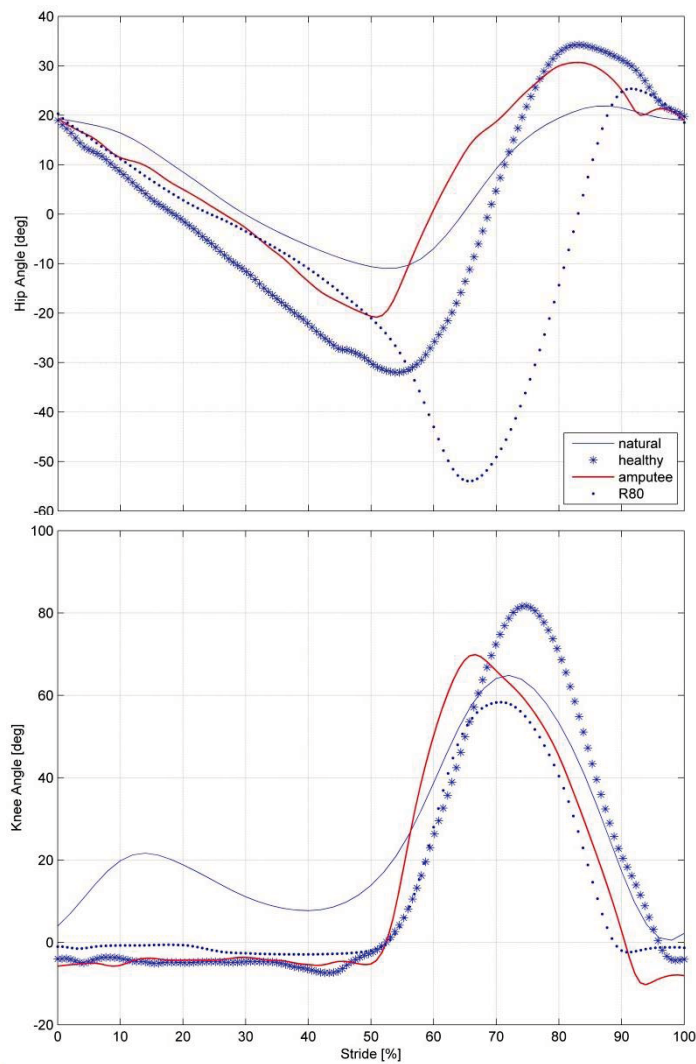
TESTS

amputee subjects



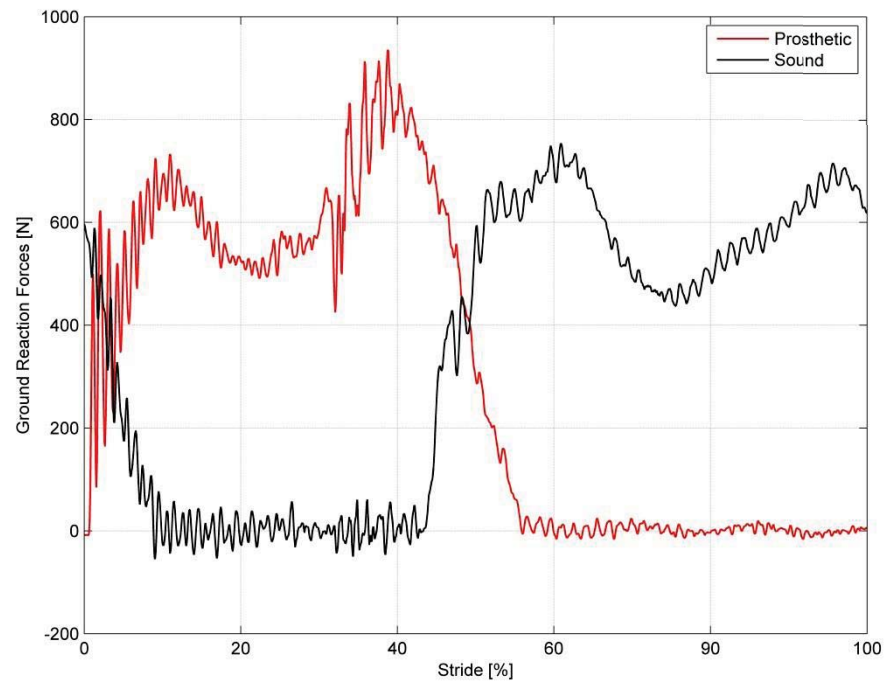
RESULTS

joint angles



RESULTS

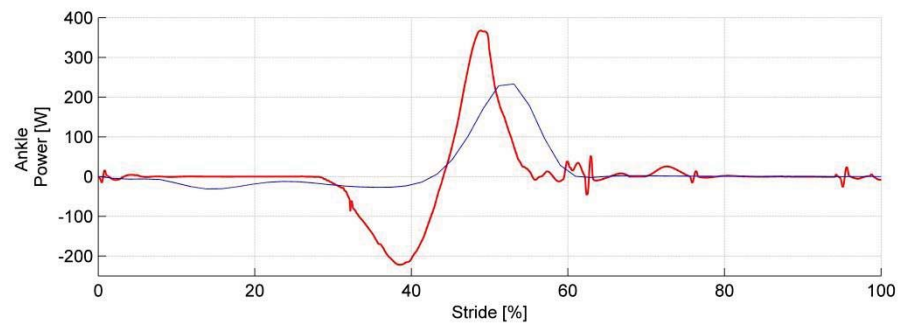
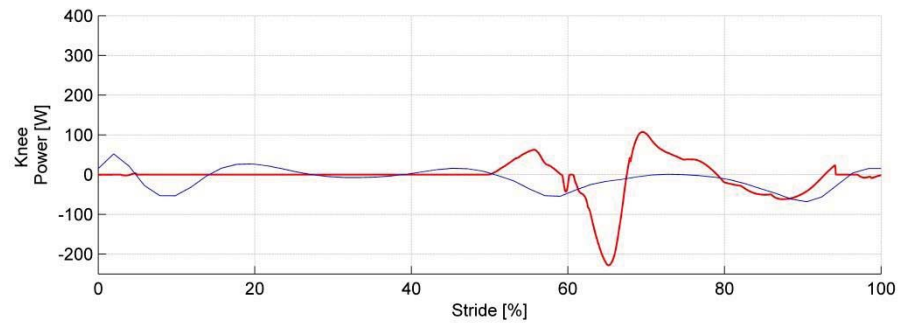
ground reaction forces



symmetric ground reaction
force behavior

RESULTS

joint power



Significant ankle
push-off generation